

# Alzheimer's Disease Pathogenesis: The Denied Access Model

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## Abstract

Currently, AD has no cure and only treatments for the symptoms exist. Modern research still debates the toxic component of AD and the exact mechanism causing neurodegeneration. A hallmark of the disease is the production of the amyloid-beta (A $\beta$ ) peptides and eventual self-assembly of these peptides into fibrils and extracellular A $\beta$  plaques. Both plaques and oligomers are proposed to be the direct cause of AD, but it remains unclear how the physical presence of these structures affect neuronal function and pathogenesis. Biomolecule aggregation is known to play a role in the pathogenesis of numerous diseases by restricting diffusion and bulk flow, and the same restriction could occur in the brain due to the dense amyloid plaques forming in the extracellular space. These plaques could prevent proper flow and diffusion of essential nutrients and prevent cellular waste removal by acting as extracellular channel blockades; however, limited models exist that address these issues. Alternative models and molecular tools need to be developed which focus on diffusion and bulk flow in relation to neural function and the physical presence of amyloid plaques. This review aims to evaluate the effect of the plaques on diffusion and bulk flow in relation to neural function in the brain.

**Keywords:** Neurodegeneration; Dementia; Amyloidosis; Protein aggregation

## Introduction

Obstruction of bulk flow by aggregated biomolecules is thought to play an important role in the pathogenesis of numerous human diseases, such as kidney stones, gallbladder stones, atherosclerosis, and thrombotic cardiovascular diseases [1]. Amyloid plaques deposited in the human brain are derived from amyloid-beta (A $\beta$ ) peptides that aggregate and form fibrils which bundle to form plaques [2]. These plaques are also made of other proteins, lipids, and their calcification. How the presence of plaques affects neuronal function and pathogenesis, and whether the amyloid plaques obstruct flow of fluid molecules is unclear. Compared to the centimeter large atherosclerotic plaques or kidney stones, amyloid plaques are smaller, often less than 50  $\mu$ m in diameter, making them a difficult subject to isolate and study.

The AD field has shifted from studying the potential toxicity of the plaques to studying the toxicity of the intermediate oligomers [3]. Some groups believe the plaques represent a non-toxic byproduct and provide a neuroprotective role by sequestering the oligomers [4-7]. After years of oligomer-focused research, numerous inconsistent results and lack of evident *in vivo* toxicity exists [8]. New methods are needed to study the potential physical toxicity of the plaques in relation to diffusion and bulk flow and to study the physical relationship of extracellular protein aggregation to viscosity and neuronal function. The cause of the massive amount of cell death found in AD remains unexplained so the search for an alternative toxicity is needed.

Aggregation and transformation of misfolded proteins into amyloid fibrils is a commonly observed phenomenon in dozens of human diseases, ranging from diabetes mellitus type 2 to neurodegenerative diseases such as Alzheimer's disease (AD), Huntington's disease, and Parkinson's disease [9]. Since the human body has no known mechanism for removing these amyloids, patients tend to already have extensive amyloid deposits once diagnosed, which leads to poor prognoses [10]. Specifically in AD, A $\beta$  accumulation with time leads to the formation of amyloid plaques [11].

Currently, the pathogenesis of Alzheimer's disease remains unknown. Two leading hypotheses have been proposed: 1) amyloid plaques are pathogenic, and more recently, 2) the oligomer intermediates or as we

refer to them, colloids, of fibril formation are pathogenic. Amyloid fibrils can further aggregate into a gel and there is a potential link between gelation and cellular death, as gels are known to eliminate bulk flow at the macroscopic level [12]. However, bulk flow at the microscopic level, under hydrostatic pressure, remains an area of study. New methods need to be developed to determine if amyloid plaques obstruct fluid flow and the circulation of nutrients, waste, and bio-signaling molecules through brain tissues and extracellular space.

## AD pathogenesis: Oligomer vs. amyloid hypotheses

Aggregation and accumulation of two different protein molecules causes pathogenesis in AD. Tau, a protein associated with cytoskeleton assembly, accumulates intracellularly to form macromolecule networks called neurofibrillary tangles (NFTs). A $\beta$ , a peptide fragment, accumulates in the extracellular space in structures called plaques. Virtually all neurons that degenerate during the development of AD have accumulation of one or both forms of aggregation; however, A $\beta$  formation alone can attribute to the disease [13].

## Amyloid beta oligomers and aggregation

Once the A $\beta$ 40 or A $\beta$ 42 peptide is produced, the exact pathways and mechanisms of amyloid aggregation at the molecular level are poorly understood, which hinders rational pharmaceutical interventions. Critical intermediates in this pathway, colloids and their linear aggregates, composed of highly ordered  $\beta$ -sheet complexes [14] were discovered using atomic force microscopy [15] and later confirmed using transmission electron microscopy [16].

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Protein molecules initially aggregate into colloidal spheres of uniform size, which then join together linearly, forming amyloid fibrils and eventual plaques (Figure 1) [17,18]. These insoluble plaques are commonly associated with cell death [3] and may lead to progressive degeneration of the blood-brain barrier (BBB) [19]. The accumulation of Aβ plaques in the extracellular space of the brain may initiate a cascade of reactions, beginning with synaptic dysfunction and ultimately resulting in apoptosis of the neuron [3,20-22]. The plaques may form around axons [23] and become associated with activated microglia and reactive astrocytes [11], which produce toxic molecules, such as cytokines, causing dysfunction of neuronal processes. Cytokines increase the inflammation of the neuron [24] and increase the production of toxic reactive oxygen species [11].

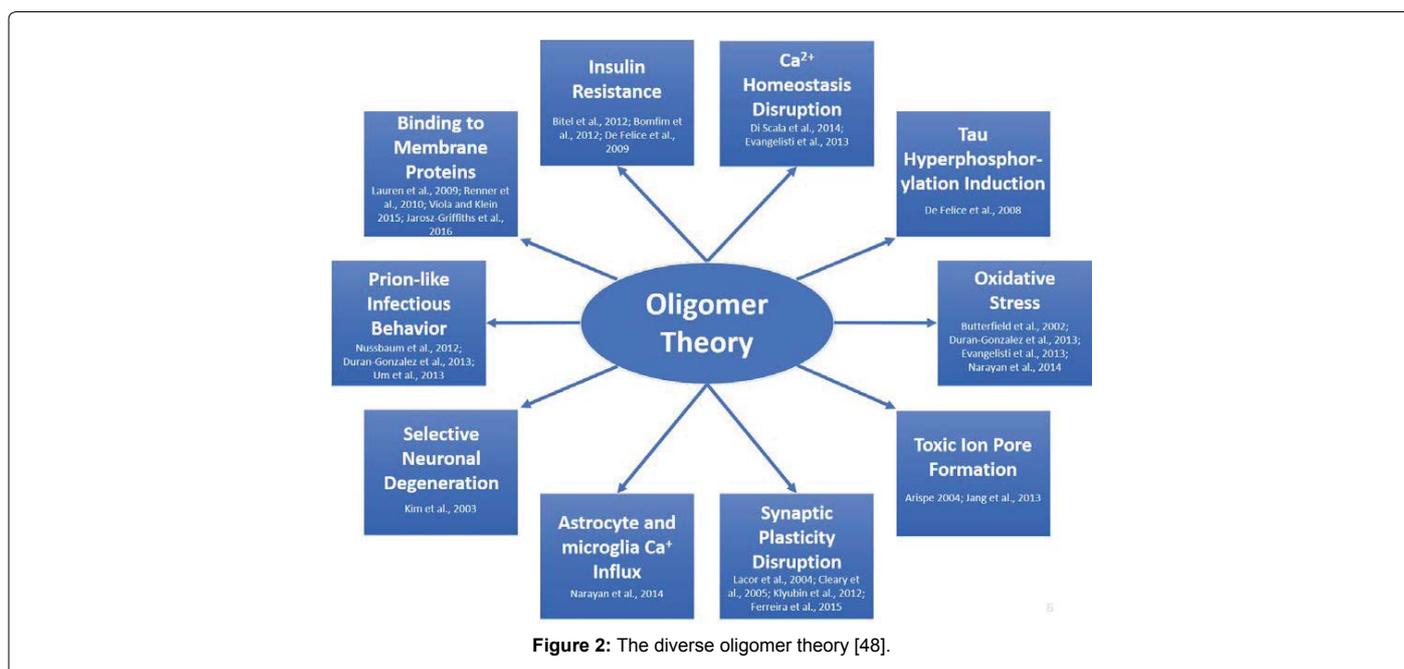
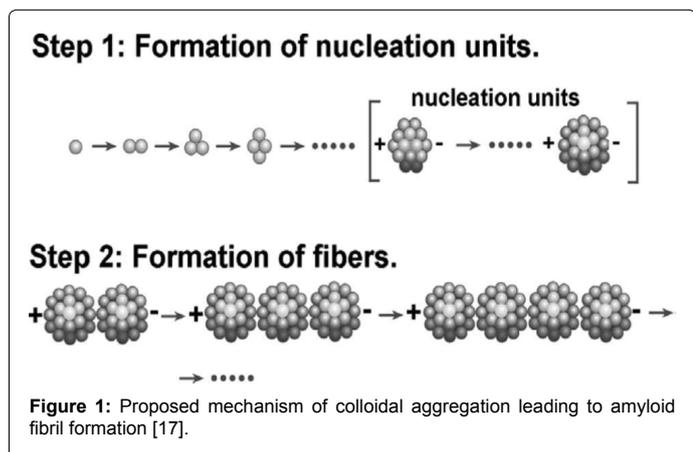
Currently, the popular amyloid cascade hypothesis (ACH), first proposed by Hardy and Higgins [25], has come under question due to formation of plaques in individuals who have normal cognitive function [26,27]. Alternatively, the oligomer hypothesis suggests the colloidal intermediates, also known as oligomers, are the toxic component that leads to neurodegeneration [28,29]. Aβ Oligomers (AβOs) are either a

step in the formation process or a byproduct of Aβ plaques [30]. The validity of the oligomer hypothesis depends on whether oligomers were present earlier than the fibrils and plaques and exercise their toxicity before substantial plaque formation. As for the ACH, plaque formation may not have followed the proposed nucleation pathway and oligomers may be a byproduct or produced by other mechanisms [30]. Interestingly, a mouse model supporting the oligomer hypothesis displayed cognitive decline before substantial plaque formation [31]; however, supporting *in vivo* work at normal concentrations is lacking. The possibility also exists where the plaques provide a neuroprotective role [32] or are simply an innocent bystander in cell death.

The main issue with the oligomer hypothesis is the diversity of toxicity (Figure 2). Countless articles are published which present new mechanistic hypotheses of AβO toxicity. To briefly summarize, AβOs have been linked to AD in the following ways: Oxidative stress and lipid peroxidation in neurons [33-36] toxic ion pore formation on the cell membrane [37,38], synaptic plasticity disruption [39-42], astrocyte and microglia calcium influx [36], selective neuronal degeneration [43], prion-like infectious behavior [34,44,45], binding to numerous membrane proteins [46-49], insulin resistance [50-52] calcium homeostasis disruption [35,53] and tau hyperphosphorylation induction [54]. One of the main issues is that AβOs lack a common description of structural toxicity and are thought of as “an emperor in need of clothes” since they possess numerous conformations ranging from monomers, to trimers, and to eventual fibrils [8]. Moreover, not all oligomers promote toxicity [54,55] and “relevant Aβ toxicity has barely been demonstrated” [56].

If AβOs are the toxic component, the massive cell loss, role in cognitive alterations and existence in non-AD patients cannot be fully explained [8]. More *in vivo* work using naturally occurring concentrations of AβOs along with other models of toxicity must be examined. Also, if they are toxic at low concentrations, such as 100 nM, why is toxicity specific to neurons and not elsewhere in the body where AβOs are also found?

The failure of many clinical trials following the ACH has caused



researchers to change focus towards the oligomer theory. Most of the failures are due to the pitfalls of the transgenic mouse AD models and their inability to successfully correlate clinical trials to the complex human system [57,58]. Interestingly, the only FDA approved clinical drugs were never tested in the transgenic mouse model [57].

The ACH is also very unappealing for therapeutic treatment [59], since even if clearance of the plaques is successful, the surrounding neurons are already dead or damaged, so cognition cannot be restored. From a clinical view, attacking the oligomers seems appealing, and has made them the key drug target [60] and the focus of recent proposals. Clinical trials targeting oligomers have also failed across the board, again likely linked to the imperfect mouse model; however, trials have not focused on all aspects of the disease. Future trials must focus on all aspects including oligomers, fibrils, plaques, and even tau [61]. Although some groups believe it, the plaques should not be considered a non-toxic byproduct, and should remain as a research focus based on their potential physical toxicity. Since existing models have not been successful, new models and methods must be proposed to address the issue of plaque's physical presence. Much debate remains as to which aggregation state is toxic to the cells [62] and more work elucidating the physical effects of plaques within the brain must be performed. Is it possible that Denied Accessed Model the two disease states are linked, and both play a role in toxicity?

#### Why denied access model?

*In vitro*, amyloid fibers have been found to be capable of further aggregating and forming gels [12,64]. Gels are known to be capable of eliminating bulk flow and reduce diffusion. Can amyloid plaques in AD be gels of porous matrix? TEM images of amyloid plaques either in AD tissue or isolated by density gradient centrifugation reveal these plaques are biogels with dense fiber network [64,65]. A transformation of brain fluid to a gel-like state due to amyloid fibril formation could have drastic neurophysiological effects on viscosity-dependent processes and tortuosity, or obstructive geometry, of the extracellular space.

#### Denied access model

When surrounded by amyloid plaques/protein gel, neurites are denied to have free access to interstitial ions, nutrients, signaling molecules and metabolic waste drainage pathways, which results in the inhibition of the compound action potential propagation. This is an alternative model for the AD community to consider, although continued investigations are required to verify the model and to fulfill the details. We hypothesize that gel formation around axons may inhibit the heart-pulse-driven fluid flow and then the circulation of nutrients and ions around the axon and affect the propagation of the action potential.

#### Denied access model explains numerous observations associated with ad tissue analysis

In Alzheimer's disease, extensive neuronal cell death is found in anatomical regions of the brain where there is no presence or accumulation of neuritic senile plaques, and/or paired-helical filaments (PHF). Based on our model, plaques wrapped around axons may affect the vitality of the neuronal cell bodies located in a different anatomical region. Cognitive impairment and the degree of dementia do not correlate with the A $\beta$  plaques burden in many Alzheimer's disease patients. However, the A $\beta$  plaque burden is quantified not based on the type of the plaque but rather a sum of all types. Based on our model, primitive plaques may not change the bulk flow or viscosity as much as the classical plaque. Thus, there exists a possibility that the classical

plaque burden correlates better with the stages of Alzheimer's disease. Our model also explains the observation that in transgenic mice amyloid plaques, although not classical ones, are found, but neuronal and synapse loss are rather minimal.

The denied access model also applies to other diseases where accumulation of protein aggregates may affect local diffusion, bulk flow, and bioenergy-driven transportation. Since the toxic effect is physical rather than chemical, the model applies to not only AD but also alpha-synuclein aggregation-induced Parkinson's disease, aggregation of prion protein induced transmissible spongiform encephalopathies, and islet amyloid polypeptide aggregation induced death of the beta cell in type II diabetes. Movement of molecules, ions, and subcellular particles will all be affected due to the aggregation of proteins and then gelation of the amyloid fibers.

The denied access model is simple and inclusive of the physics and engineering perspective of gels or plaques, in addition to the biochemical nature. The inclusion of physical properties such as bulk flow and diffusion is seen in the illustration of atherosclerosis, thrombosis, gallbladder stones, and kidney stones, where aggregation of biomolecules, large and small, is also an early event of disease pathogenesis. The transportation phenomenon, or bulk flow and diffusion, through gels are an active research area in engineering.

#### Denied Access by Attenuated Diffusion and Bulk Flow Through the Amyloid Plaque

The extracellular space (ECS) defines the channel-like environment where interstitial fluids (ISF), consisting of nutrients, neurotransmitters, signaling molecules, ions, and wastes, travel through the tissues to maintain cellular homeostasis and function. The widths of the channels range from 20-40 nm and encompass around 20% of total brain volume [66,67]. Variations of the ECS geometry and volume fraction can arise during sleep, development, aging, and neurological disorders, so understanding any alterations in function are vital for neurological research and drug delivery. These variations can affect proper clearance routes, cellular uptake, diffusion, and flow of nutrients and waste across the BBB [68].

#### Diffusion

Diffusion is the net movement of individual molecules down a concentration gradient due to random motion or thermal movement. Diffusion was first defined by Adolf Fick (Eq. 1) in the 19<sup>th</sup> century as,

$$J = -D \frac{dC}{dX} \quad (1)$$

Where  $J$  is the flux through an area,  $D$  is the diffusion coefficient,  $dC$  is the change in concentration of material, and  $dX$  is the change in distance. Thus, flux is proportional to the concentration gradient. Diffusion through the ECS is determined by the volume fraction or porosity, defined as  $\alpha$  (Eq. 2) and the tortuosity or obstructive geometric capabilities of the environment, defined as  $\lambda$  (Eq. 3) [68]. Volume fraction is defined as,

$$\alpha = \frac{V_{ECS}}{V_{Tissue}} \quad (2)$$

where  $V_{ECS}$  is the volume of the extracellular space devoid of matrix components and  $V_{Tissue}$  is the volume occupied by the tissue, and tortuosity is defined as,

$$\lambda = \sqrt{\frac{D_f}{D^*}} \quad (3)$$

where  $D_f$  is the free diffusion coefficient and  $D^*$  is the effective

diffusion coefficient, typically determined using radiotracers or fluorescent dyes. The volume fraction of the ECS has been well studied using electron microscopy and occupies approximately 20% of total brain volume [69,70]. This value has been recently debated due to the difficulty in determining the ECS volume fraction in living tissues, where there is a high likelihood of ischemia; therefore, new methods, such as *in vivo* studies using quantum dots [71] and fluorescent dyes [72], have been developed and remain an area of study.

Due to the independence between volume fraction and tortuosity, it is difficult to derive a relationship between the two. There are also many non-geometric factors such as ISF viscosity (discussed in bulk flow), molecular size, ECS channel interaction [73], and the uptake of molecules by cells or across the BBB [74]. The Nicholson group attempted to derive an empirical relationship using Archie's law (Eq.4) [75],

$$\lambda = \alpha^{-n} \quad (4)$$

The formula relates sedimentary porosity and saturation. It was determined that the values remained independent since the tortuosity exponent,  $n$ , is a variable according to the original law. However, if the tortuosity exponent is variable due to the variance between regions of white and gray matter, the relationship displays some dependence [78,79]. This relationship remains an important area of investigation when discussing diffusion throughout the brain.

### Bulk flow

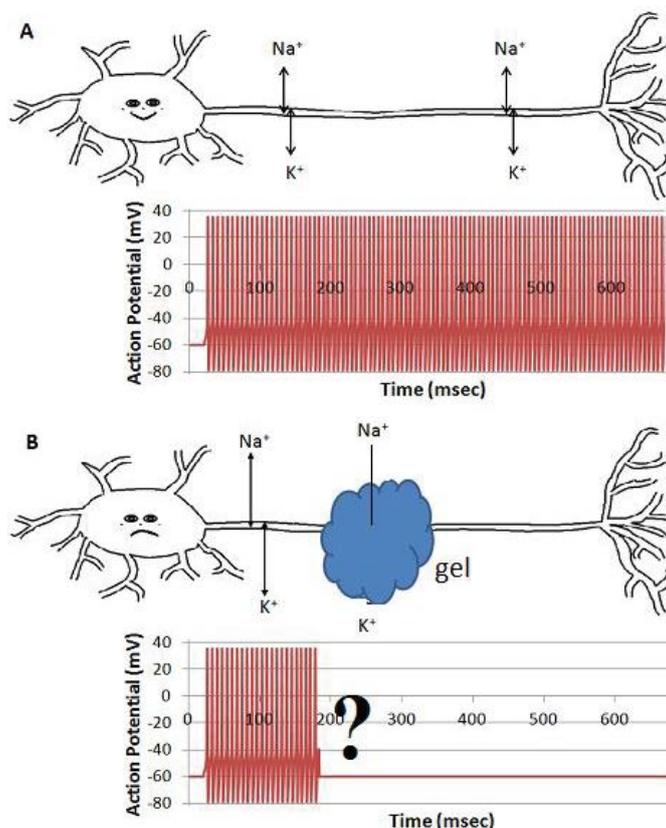
Bulk flow is the movement of water and solutes in response to a

pressure gradient. Analysis of fluid flow through a porous matrix can be defined using Darcy's flux (Eq. 5) which states,

$$Q = \frac{K_s \nabla P}{\eta} \quad (5)$$

Where  $Q$  is the flux of fluid per unit area through a porous matrix,  $K_s$  is the Darcy permeability coefficient,  $\nabla P$  is the hydrostatic pressure gradient across the matrix and  $\eta$  is the viscosity of the ISF. According to the equation, bulk flow is strongly dependent on the viscosity of the media and the permeability through a porous matrix.

The movement of fluids through the ECS of the brain has numerous implications, including cell to cell communication, drug delivery, distribution, waste clearance, ionic homeostasis, and immune function [80]. Bulk flow through the ECS remains a debated issue [81]. Flow typically occurs via osmotically balanced fluid secretion across the BBB but can also be generated as fluid secretion from cells [82] and the choroid plexuses [83]. One research group determined bulk flow only occurs in perivascular spaces surrounding capillaries and little to no flow occurs throughout the remaining ECS [84]. Varying flow rates were also found when comparing white to gray matter regions of the brain. White matter regions expressed a flow rate of 10.5  $\mu\text{m}/\text{min}$  towards the ventricles, but regions of gray matter only displayed flow under osmotic stress [85]. The issue of diffusion also returns, since some groups believe that diffusion cannot be the sole clearance mechanism due to a constant rate of clearance for various sized molecules [86-88]. However, another group that used albumin and large dextrans suggests diffusion is responsible for clearance and is independent from bulk flow



**Figure 3:** Denied access model. The neurite regions surrounded by amyloid gel plaques are denied from accessing to nutrient and signaling molecules as well as to the drainage pathways for metabolic wastes. This denied access leads to the inhibition of the action potential propagation and eventually the degeneration of the disused neurites.

[89]. As mentioned, quantitative measurements of flow rates have been made by injecting tracers into the brain and observing their movements [85,90], but no work has examined direct effects of A $\beta$  plaques.

Limited research has been conducted towards understanding how the formation of amyloid plaques affects diffusion. Researchers utilizing diffusion-weighted magnetic resonance imaging (DW-MRI) have demonstrated a reduced interstitial fluid diffusion in the brain of APP23 transgenic mice [91] and reduced diffusivity in the white matter of patients suffering from sporadic Jakob-Creutzfeldt disease [92], another neurocephalopathy associated with the formation of insoluble protein aggregates. Sykova and Colleagues [93] analyzed the ECS and the volume fraction and diffusion of the cerebral cortex in APP23 mice using real-time tetramethylammonium (TMA) and DW-MRI methods. They determined that the volume fraction increased in aged APP23 mice by approximately 3.0% in both female and male mice and apparent diffusion of TMA decreased by 7.0% in females and 1.7% in males. Plaque load was also twice as high in females as it was in males. For the control, the ECS volume fraction decreased by approximately 7% in males and 4% in females, and the apparent TMA diffusion increased by less than 1% in aged mice [93]. These results suggest that plaques may decrease diffusion by increasing overall brain tortuosity; however, the direct correlation remains unknown.

Another physical impact of plaque formations may be fluid clearance from the brain by increasing the tortuosity, as previously noted by [93]. Clearance is important across the BBB to prevent buildup of toxic molecules and to help maintain cellular homeostasis (Figure 4A). Clearance also prevents high concentrations of soluble A $\beta$  and eventual plaque formation [94,95] and an age-related imbalance of A $\beta$  release could drive the progression of AD [3]. The accumulation of plaques in the extracellular space (Figure 4B) and drainage pathways (Figures 4C and 4D) could reduce the clearance of high molecular weight substances by impeding the normal clearance routes [68,70,96,]. Plaques can become very large, up to 150  $\mu$ m in diameter [97], so it is likely that the dense plaques can restrict fluid movement through the less than 0.1  $\mu$ m extracellular space pathways. Moreover, AD patients display a significant reduction in ISF flow [98], which may be linked to the increased plaque load. Future work must develop new methods

to evaluate the effect of the presence of amyloid plaques on neuronal function and fluid flow in brain tissue.

### Techniques for the study of amyloid plaques on neuronal function

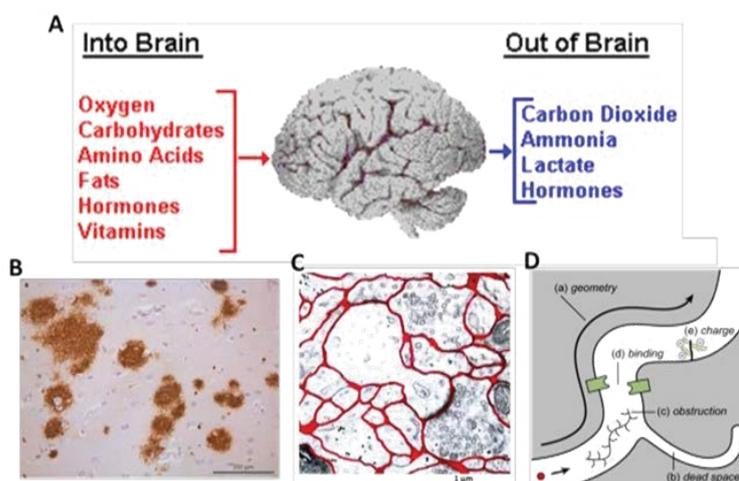
We identified four new methods being developed in our laboratory to study if and how the amyloid plaque affects the neuronal function. Specifically, these methods are:

#### Fibrin as an A $\beta$ plaque proxy

To study the effect of amyloid plaque on neuronal function, we need to have the plaque prepared in the presence of the functional neurons, under physiological conditions and within seconds to minutes. The constraints of the physiological condition and the short time period force us to look for a proxy of amyloid fibril gel as they take hours to days to produce, often under non-physiological conditions.

**Volume fraction and pore size:** Ideally, the use of A $\beta$  is preferred, but time, attainability, and practicality must be considered. Fortunately, amyloid fibrils are not the only example of a fibrous network created by proteins. The hindrance of diffusion and convective transport are also elementary properties of wound healing, a process that relies on blood clotting due to the formation of a fibrin gel network. Fibrin gels are formed within a few minutes between the interactions of the protein fibrinogen, from blood plasma and the activating enzyme thrombin [99]. Thrombin cleaves fibrinopeptides located in the middle of fibrinogen, producing a fibrin monomer and subsequent protofibril formation [100]. Compared to amyloid gels, fibrin is easily attainable, found within the body, and forms rapidly under physiological conditions [99]. Amyloid gels, on the other hand, require hours or even days to form *in vitro*. Importantly, fibrin is physically similar to amyloid gels and provides an ideal proxy. With these factors considered, a convenient analog to study the physical effects of toxicity must be used. This would allow for rapid and feasible studies of protein aggregation in cellular environments.

Fibrin provides an ideal analog for studying the physical effects of amyloid plaques or gels and the potentially abolished bulk flow on



**Figure 4:** Bulk flow and fluid clearance in the brain. (A) Nutrients and toxins must be able to freely move into and out of the brain (Image from the University of New Hampshire). (B) Plaque formations can become very large, up to 150  $\mu$ m in diameter [97] and can likely block the (C) less than 0.1  $\mu$ m extracellular channels and synaptic junctions [70]. (D) Factors within the extracellular space such as charged residues, binding, and dead space can also affect fluid flow [68].

neuronal function; however, the gel must have the appropriate porosity to simulate the amyloid plaque. To qualify, fibrin gel must have higher porosity compatible to amyloid gel. Scanning electron microscopy (SEM) (Figure 5A) and atomic force microscopy (AFM) (Figure 5B) images reveal a dense fibrous network with pore sizes less than 1  $\mu\text{m}$ , which are comparable to A $\beta$  (Figure 5C).

Chemically, fibrin is different from A $\beta$ , and although fibrin is not a true amyloid, its regulation is similar to the enzymatic control of peptide hormone aggregation [101]. Fibrin has a high  $\beta$ -sheet content of 40% [102] and can stain using Congo red [103], an amyloid-specific stain. Kranenburg and colleagues [103] believe fibrin can form cross- $\beta$  structures and amyloid fibrils, and that these  $\beta$ -sheet structures function as the scaffold to activate plasmin, which eventually cleaves aggregated fibrin.

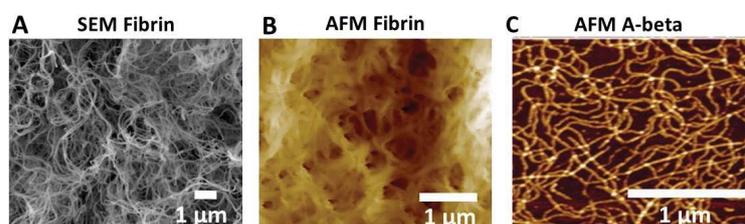
**Viscosity of gels using molecular rotors:** Increased viscosity is also thought to play a role in the pathogenesis of AD linked to amyloid plaque formation. De la Torre and Mussivand [19] hypothesized that blood viscosity can increase due to amyloid deposits causing degeneration of brain capillaries at the BBB; however, the link between increased local viscosity and degeneration has remained elusive. Protein aggregation into a gel, as seen *in vitro*, possibly also occurs *in vivo*.

Bulk viscosity is known to be different from molecular viscosity. For fibrin to be qualified as an amyloid fibril gel proxy for diffusivity study, the viscosity of fibrin gel, at the molecular level, needs to be

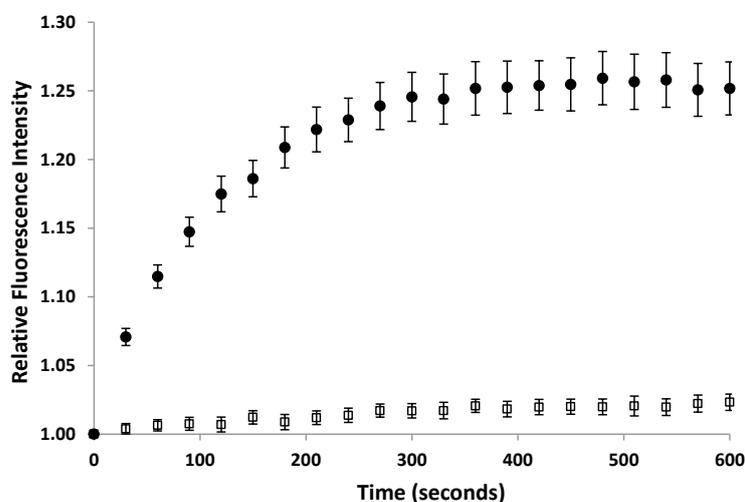
comparable or lower than that of amyloid fibril gel. To study ion or molecule diffusion across the amyloid plaque, the molecular viscosity is of interest. A successful technique used to study viscosity applies fluorescent molecules known as molecular rotors. These rotors are able to alter their fluorescence by changing conformation [104,105]. This rate of change is dependent on the microviscosity of the environment. Decreasing bond rotation increases fluorescent yield [106]. Previous work in the lab used 9-(2-carboxy-2-cyanovinyl) julolidine (CCVJ) as the molecular rotor to determine how the formation of fibrin altered medial viscosity [107]. Results were compared to varying concentrations of glycerol, a known viscous solution, where increasing concentrations amplified the fluorescence intensity. In 20 mg/ml fibrin, fluorescence intensity increased during gelation with the greatest increase occurring within the first 60 s. Only a small increase occurred in 10 mg/ml fibrin (Figure 6), suggesting 20 mg/ml would be an optimal concentration to study gelation in a time dependent manner. This work established that gelation results in an increased microviscosity.

### Sciatic nerve as a CNS proxy

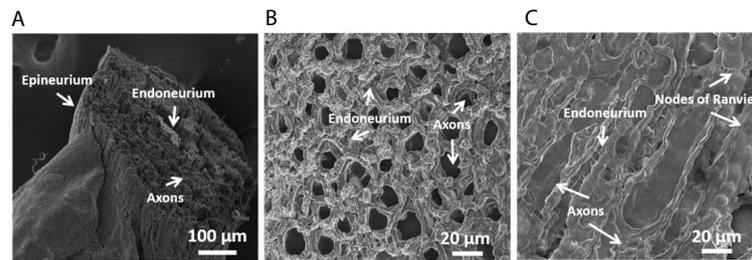
A goal is to determine whether the physical presence of plaques causes toxicity. Since *in vivo* experiments using mice or human models are difficult to perform, an ideal analog is the sciatic nerve from frogs, such as the *Xenopus laevis*, as it has long been successfully employed in studying numerous physiological properties of axons and is well characterized. The sciatic nerve is a large bundle of many axons surrounded by an epineurium membrane (Figure 7A). The



**Figure 5:** Scanning electron micrograph of fibrin (A), atomic force micrograph of fibrin (B), and atomic force micrograph of amyloid-beta (C). Fibrin was generated using a 10:1 ratio of fibrinogen (20 mg/ml in 0.9% NaCl) and thrombin (50 U/ml in 0.1% BSA, pH 7.4). Amyloid fibril formation of 50  $\mu\text{M}$  A $\beta$ 42 fibrils incubated at 37°C is seen in 1 week [128].



**Figure 6:** Relative fluorescence intensity of 5  $\mu\text{M}$  CCVJ in two different fibrin gels. One gel was composed of 20 mg/mL fibrinogen ( $\bullet$ ), and the other was composed of 10 mg/mL fibrinogen ( $\square$ ). Thrombin concentration was kept constant (10-75 U/mL).



**Figure 7:** Scanning electron micrograph images of *Xenopus laevis* sciatic nerve. (A) The sciatic nerve image was generated by fixing the nerve bundle in 3% glutaraldehyde, washing in 0.1% PBS, staining in 1% osmium tetroxide/0.1% PBS, dehydrating in increasing concentrations of ethanol and ethyl-acetate, and critical point drying. Cryostat sections were also prepared in the cross sectional (B) and longitudinal (C) directions at 20 μm thickness.

individual axons are structurally supported with collagen, known as the endoneurium, and encompassed with myelin containing nodes of Ranvier (Figures 7B and 7C), which allows for rapid conduction of action potentials.

In AD, white matter atrophy due to plaque formation may be as important as gray matter atrophy. Plaques are more numerous in associative regions of the brain higher in gray matter content, such as the extracellular matrix of the hippocampus where learning and memory take place [108] and where the most severe neuropathological changes occur [22]; however, plaques are also found in myelinated white matter regions such as the cortex. The question arises as to whether the myelinated sciatic nerve would serve as an appropriate proxy for neurodegenerative studies. Although the gray matter regions are more intensely studied, white matter atrophy occurs in AD [109] and is found in roughly 60% of AD cases [110]. White matter atrophy is often considered secondary to gray matter damage [111], but recent developments determined white matter damage occurs in pre-AD stages and cannot be linked to gray matter atrophy [112,113]. Furthermore, studies analyzing white matter attributed the damage to cognitive decline [114] and discovered higher levels of soluble A $\beta$  in AD patients [115].

Many physiological experiments using the frog sciatic nerve have been conducted examining the compound action potential (CAP) and the biochemical effects that may cause degeneration. One group examined the time-dependent effects acrylamide had on the anti-oxidative stress in rat nerve tissues. With increased concentrations injected into rats over a few weeks, decreases were found in both CAP duration and CAP amplitude [116]. Furthermore, they found that acrylamide may be associated with an increase in lipid peroxidation and reduction of the anti-oxidative capacity. Another experiment examined the direct effects of polyethylene glycol (PEG) on isolated rabbit sciatic nerves [117]. They found 40% PEG abolished the compound action potential within an hour due to increased osmotic pressures creating a hypertonic environment and shrinkage of the axon. These structural changes may lead to reduced ion permeability, neuronal stress, and eventually neuronal death [117]. These results suggest the frog sciatic nerve may be an ideal tissue for neurophysiology experiments to test the effect of viscosity on neuronal function. Completing these experiments on gray matter would be difficult; whereas, the sciatic nerve is easy to dissect and shares common physiological features as central nervous system neurons [118]. If plaques are the culprit for neuronal loss, similar reasons for toxicity may be seen in both white and gray matter.

### Quantifying diffusion through plaques and brain tissue

How amyloid plaques affect the circulation of nutrients, wastes and biosignaling molecules in brain tissue remains unknown. Molecules

move through a matrix either by diffusion driven by Brownian motion, or carried by fluid movement or bulk flow. Thus, methods are needed to analyze diffusion and bulk flow. FRAP is a straightforward technique developed to study molecular diffusion in media [119]. Using a confocal laser scanning microscope (CLSM), a user-defined region of interest is selected and bleached, leaving the surrounding area unbleached [120]. With time, the unbleached molecules diffuse into the bleached area and exchange with the bleached molecules [121,122]. Using one of many possible fluorescent dyes, such as rhodamine B (RhoB) or fluorescently tagged proteins, a fluorescent recovery curve can be generated and a diffusion coefficient of the dye through the sample can be calculated [123,124].

Protocols and data analysis of FRAP experiments differ between laboratories causing the existing body of data to be incomparable [125]. Many finite factors affect diffusion, suggesting that each lab must perfect their own calibrations and controls. Numerous studies using this technique and a variety of fluorophores have been completed; however, one vital element of experimental approach arises, fixation of the tissue. Most FRAP experiments analyze real-time protein movement and interactions requiring live tissue samples and cell cultures. If the methods advance for fixed tissue, countless studies could be completed and experimental procedures would be simple.

### Effect of plaques on bulk flow

The physical presence of amyloid plaques may hinder brain clearance of waste and the movement of nutrients. At the tissue level, experiments injecting molecular tracers [85,90] and studies using positron emission tomography [98] have evaluated bulk flow, but they are difficult to perform for standard laboratories. These experiments were focused on movement of fluid into and out of the brain rather than through specific regions. Other experiments focused on either CSF or ISF production rates in relation to bulk flow [126] or used computer based modeling to analyze flow [127]. Feasible, reliable, and straightforward techniques are needed to study fluid movement at the cellular level and how the plaques affect the flow.

It is possible to estimate the bulk flow if the diffusion coefficient of a particular molecule is known through a plaque and free medium. Knowing these will allow the tortuosity and void volume fraction of the plaque to be estimated. That information can then be used to estimate Darcy's permeability through the plaque and the effect on bulk flow compared to normal flow through the ECS. The Diffusion coefficient can be derived from FRAP experiments.

### Conclusion

Gelation and the increased viscosity and reduced bulk flow is a common phenomenon in physical chemistry and engineering, but

the increased viscosity has never been confirmed in A $\beta$  plaques found in AD. *In vitro*, proteins, such as A $\beta$  and lysozyme, can undergo conformational changes and self-assemble into amyloid fibrils. Eventually these fibrils can aggregate and form highly viscous, rigid gels [12,63]. *In vivo*, it is likely that amyloid plaques act as viscous and structured gels. The elimination of bulk flow and reduced diffusivity due to plaque formation in the ECS near axons may be responsible for the inhibition of action potential propagation, which, in time, may cause neuronal death. Here we introduce the denied access model: when surrounded by amyloid gel plaques, neurites are denied access to nutrients, signaling molecules, and metabolic waste drainage pathways, eventually leading to neurotic dystrophy. This is an alternative model for the AD community to consider, although continued investigations are required to verify the model and to fill in the details.

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